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18-01-2019	)		Final Report		15-Apr-2014 - 31-Jan-2018	
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Final Repo	rt: The Spatiot	emporal Reso	lution of Cognitive	W911	W911NF-14-1-0173	
Signals Revealed Through High-Density uECoG Mapping			5b. GR	5b. GRANT NUMBER		
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UU	υυ υυ		UU		19b. TELEPHONE NUMBER 215-898-7504	

#### **RPPR Final Report**

as of 24-Jan-2019

Agency Code:

Proposal Number: 63033LS Agreement Number: W911NF-14-1-0173

**INVESTIGATOR(S):** 

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**Phone Number: 2158987504** 

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Country: USA

DUNS Number: 042250712 EIN: 231352685

Report Date: 30-Apr-2018 Date Received: 18-Jan-2019

Final Report for Period Beginning 15-Apr-2014 and Ending 31-Jan-2018

Title: The Spatiotemporal Resolution of Cognitive Signals Revealed Through High-Density uECoG Mapping

Begin Performance Period: 15-Apr-2014 End Performance Period: 31-Jan-2018

Report Term: 0-Other

Submitted By: YALE COHEN Email: ycohen@mail.med.upenn.edu

Phone: (215) 898-7504

**Distribution Statement:** 1-Approved for public release; distribution is unlimited.

STEM Degrees: 0 STEM Participants: 1

Major Goals: The spatiotemporal resolution of the neural code that underlies attention (and other cognitive signals) is not well understood, despite a large literature that tests how these signals are modulated at the level of the single neuron. These issues have not been resolved because, until recently, it was not possible to record from large numbers of brain sites simultaneously. The goal of this grant is to fill our knowledge by testing two hypotheses. First, attentional signals can be decoded from μΕCoG signals in the ventrolateral prefrontal cortex (νPFC), which is cortical region that is functionally involved in auditory attention. Second, the ability of a Bayesian linear estimator to decode attentional signals depends on the spatiotemporal resolution of the μΕCoG-array signals.

Accomplishments: 1. designed and produced a uECoG device

- 2. implanted uECoG device in PFC of rhesus monkey
- 3. recorded successfully uECoG signals from device
- 4. Demonstrated that both sensory and cognitive (i.e., choice dependent) signals can be read out from uECoG signals.
- 5. Our modular system shows stable long-term recordings (~1 year) as the decoding accuracies are not varying much across the implantation period.
- 6. Determined that sufficient coverage and recording resolution is needed for accurate "decode".

Training Opportunities: Nothing to Report

**Results Dissemination:** 1. Abstract at 2018 Society for Neuroscience Meeting: Chiang, J., Lee, J., Williams, A. J., Cohen, Y. E. & Viventi, J. in Neuroscience 2018 Vol. Program No. 431.21 Online (Society for Neuroscience, San Diego, CA, 2018).

2. Preparing manuscript for submission in early 2019 to IEEE journal.

Honors and Awards: Nothing to Report

**Protocol Activity Status:** 

**Technology Transfer:** Nothing to Report

**PARTICIPANTS:** 

#### **RPPR Final Report**

as of 24-Jan-2019

**Funding Support:** 

**Funding Support:** 

**Funding Support:** 

**Funding Support:** 

Participant Type: PD/PI Participant: yale cohen

Person Months Worked: 1.00

Project Contribution: International Collaboration: International Travel:

National Academy Member: N

Other Collaborators:

Participant Type: Co PD/PI Participant: jonathan vivienti Person Months Worked: 1.00

Project Contribution: International Collaboration: International Travel:

National Academy Member: N

Other Collaborators:

Participant Type: Technician Participant: harry shirley Person Months Worked: 1.00

Project Contribution: International Collaboration: International Travel:

National Academy Member: N

Other Collaborators:

Participant Type: Graduate Student (research assistant)

Participant: chia han chiang Person Months Worked: 1.00

Project Contribution: International Collaboration: International Travel:

National Academy Member: N

Other Collaborators:

#### **CONFERENCE PAPERS:**

Publication Type: Conference Paper or Presentation Publication Status: 1-Published Conference Name: 36th Annual International Conference of the IEEE Engineering in Medicine and Biology

Society

Date Received: 25-Aug-2016 Conference Date: 27-Aug-2014 Date Published: 27-Aug-2014

Conference Location: chicago, IL

Paper Title: A low-cost, multiplexed electrophysiology system for chronic uECoG recordings in rodents

Authors: Wang, J., Trumpis, M., Insanally, M., Froemke, R., & Viventi, J.

Acknowledged Federal Support: Y

#### **RPPR Final Report**

as of 24-Jan-2019

Publication Type: Conference Paper or Presentation Publication Status: 1-Published

Conference Name: 7th Annual International IEEE EMBS Conference on Neural Engineering

Date Received: 07-Mar-2017 Conference Date: 22-Apr-2015 Date Published: 24-Apr-2015

Conference Location: Montpellier, France

**Paper Title:** A low-cost, 61-channel µECoG array for use in rodents.

Authors: Woods, V., Wang, C., Bossi, S., Insanally, M., Trumpis, M., Froemke, R., & Viventi, J.

Acknowledged Federal Support: Y

Publication Type: Conference Paper or Presentation Publication Status: 2-Awaiting Publication

Conference Name: 8th Annual International Conference of the IEEE Engineering in Medicine and Biology

Society

Date Received: 29-Aug-2016 Conference Date: 16-Aug-2016 Date Published: 16-Aug-2016

Conference Location: Orlando, FL

Paper Title: In vitro Assessment of Long-Term Reliability of Low-Cost ?ECoG Arrays

Authors: Kay Palopoli-Trojani Virginia Woods, Chia-Han Chiang, Michael Trumpis, and Jonathan Viventi

Acknowledged Federal Support: Y

Publication Type: Conference Paper or Presentation Publication Status: 1-Published

Conference Name: Society for Neuroscience, 2018

Date Received: 16-Jan-2019 Conference Date: 05-Nov-2018 Date Published: 03-Nov-2018

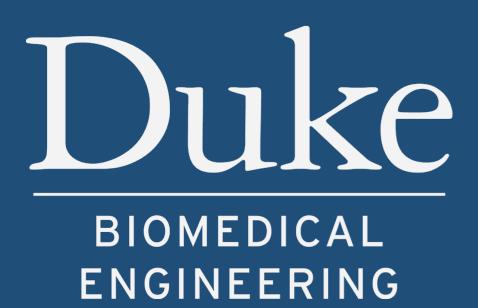
Conference Location: San Diego, CA

Paper Title: A modular high-density 294 channels uECoG system on macaque vIPFC for auditory cognitive

decoding.

Authors: C. CHIANG, J. LEE, C. WANG, A. J. WILLIAMS, Y. E. COHEN, J. VIVENTI

Acknowledged Federal Support: Y



# A modular high-density 294 channels µECoG system on macaque vlPFC for auditory cognitive decoding



C. Ken Chiang<sup>1</sup>, Jaejin Lee<sup>2</sup>, Charles Wang<sup>1</sup>, Ashley J. Williams<sup>1</sup>, Yale E. Cohen<sup>2,3</sup>, and Jonathan Viventi<sup>1</sup>

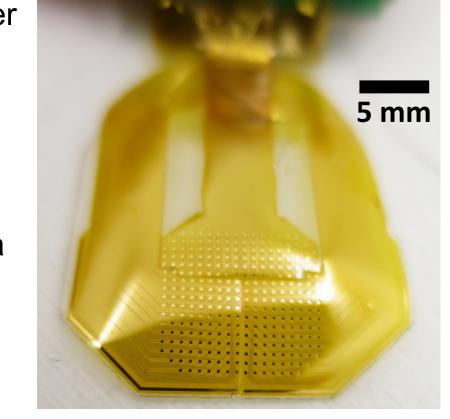
<sup>1</sup>Department of Biomedical Engineering, Duke University <sup>2</sup>Department of Otorhinolaryngology, University of Pennsylvania <sup>3</sup>Department of Bioengineering, University of Pennsylvania <sup>3</sup>Department of Bioengineering, University of Pennsylvania <sup>4</sup>Department of Bioengineering, University of Pennsylvania <sup>5</sup>Department of Bioengineering, University of Pennsylvania <sup>6</sup>Department of Bioengineering, University of Pennsylvania <sup>7</sup>Department of Bioengineering, University of Pennsylvania <sup>7</sup>Department of Bioengineering, University of Pennsylvania <sup>8</sup>Department of Bioengineering, University of Pennsylvania <sup>9</sup>Department of Bioengineering, University of Bioengineering, University of Bioengineering, University of Bioengineering, U

#### INTRODUCTION

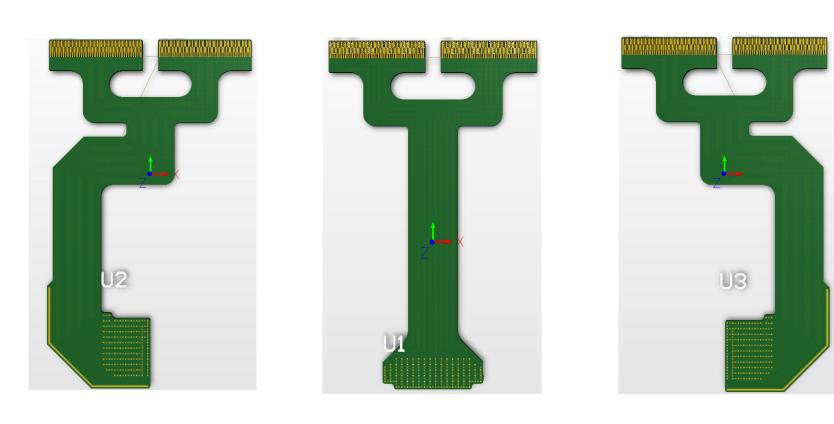
- Detecting and discriminating auditory stimuli is a complex neurocomputational problem because the stimuli of interest in the real world change simultaneously along multiple dimensions and are often mixed together with other environmental stimuli.
- It is not well understood how the brain transforms a mixture of acoustic stimuli into distinct perceptual representations.
- Auditory perceptual decisions are believed to be mediated by the ventral auditory pathway, which includes the ventrolateral prefrontal cortex (vIPFC) at its apex.
- However, the spatiotemporal resolution of the neuronal code that underlies perception and cognition in vIPFC is still unclear; and until recently, it was not possible to record from large numbers of brain sites simultaneously.
- In this work, we developed a modular, high-resolution, electrode array with long-term viability to study the information that could be decoded from vIPFC microelectrocorticographic (µECoG) signals during an auditorydetection task.

#### ELECTRODE DESIGN

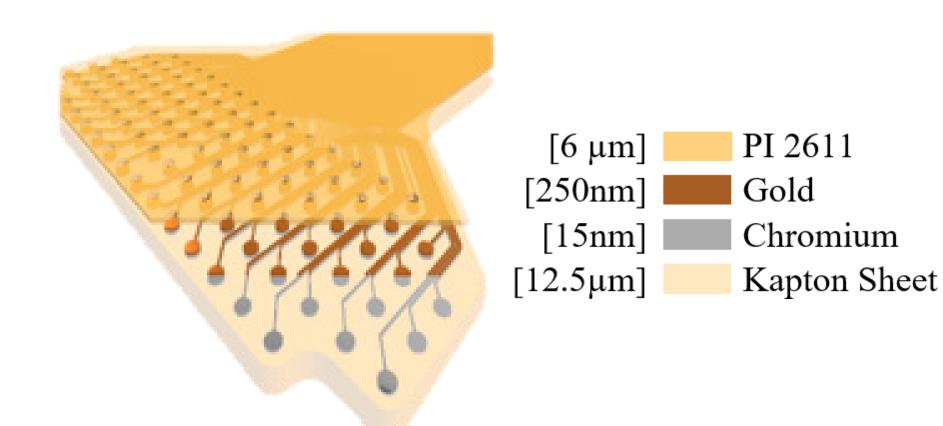
- 3 subarrays molded together
- 294 channels total
- 17 x 18 grid
- 610 µm pitch
- 229 µm (dia.) pad
- 10.4 x 11 mm<sup>2</sup> sensing area
- ~30µm thick total
- High density ZIF connector



#### Modular design

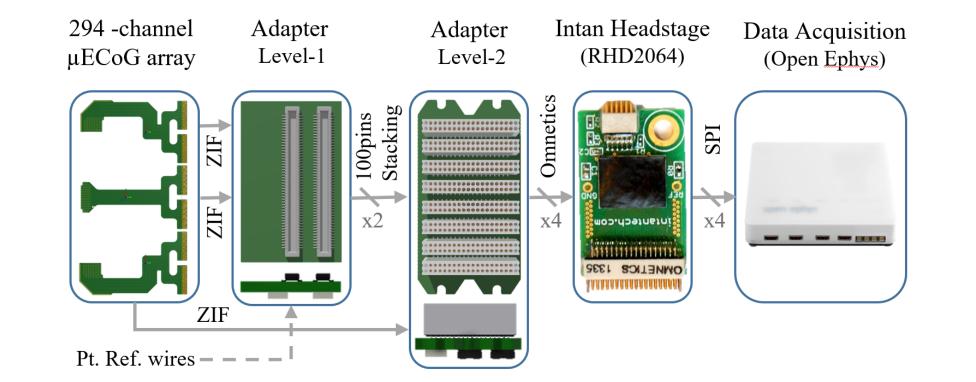


### Stack-up



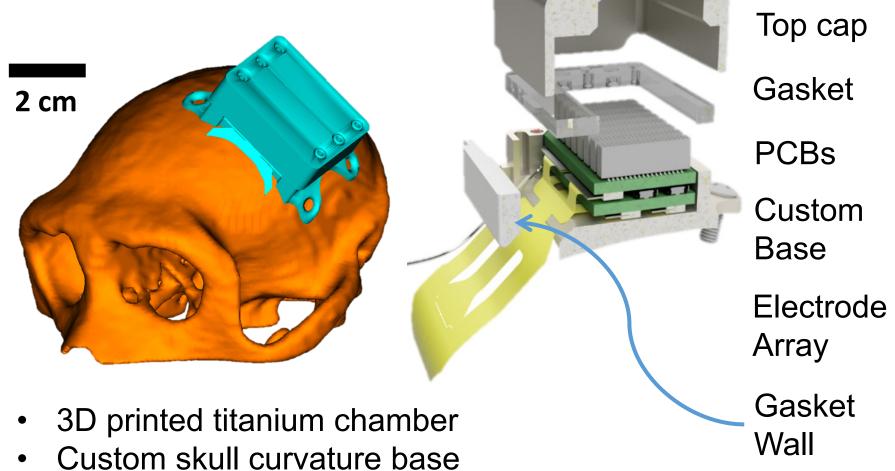
#### SYSTEM DESIGN

#### Electrical



## Mechanical

Weight: 76g

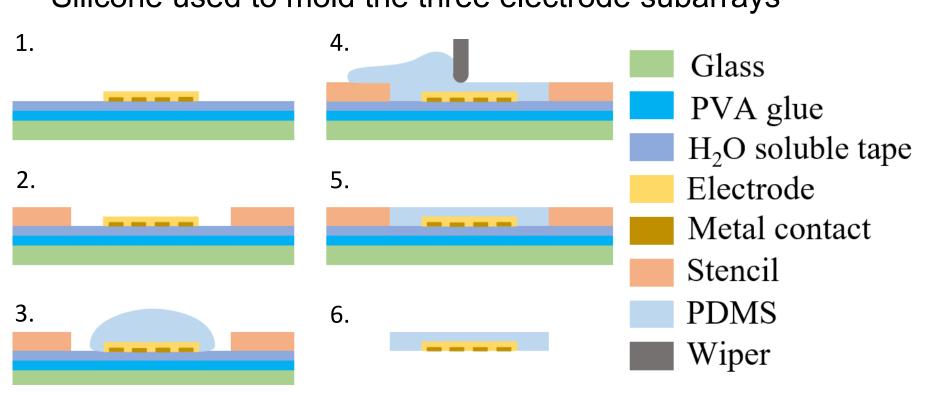


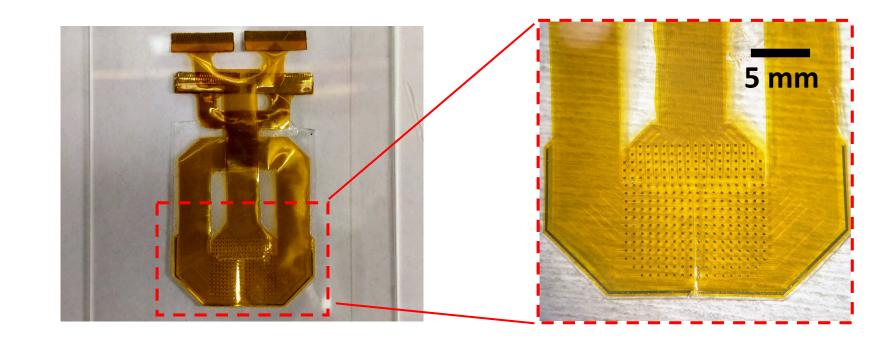
#### Molding

#### **Electrode Molding**

Overall size: 35mm x 27mm x 18mm

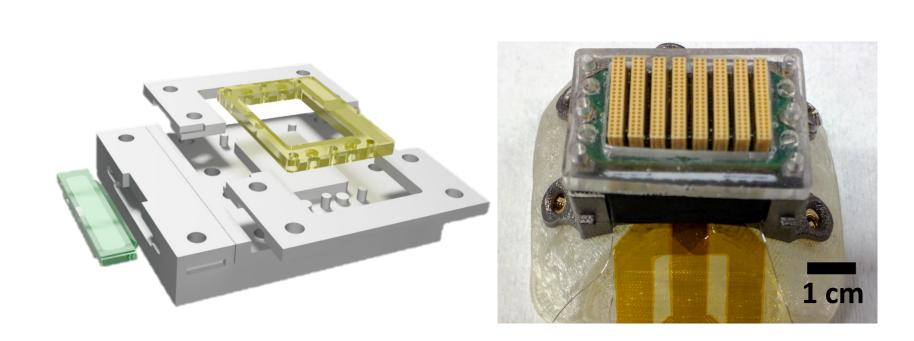
Silicone used to mold the three electrode subarrays





#### Gasket Molding

 To make the chamber water tight, we molded a gasket with PDMS and the electrode entrance wall with Sugru

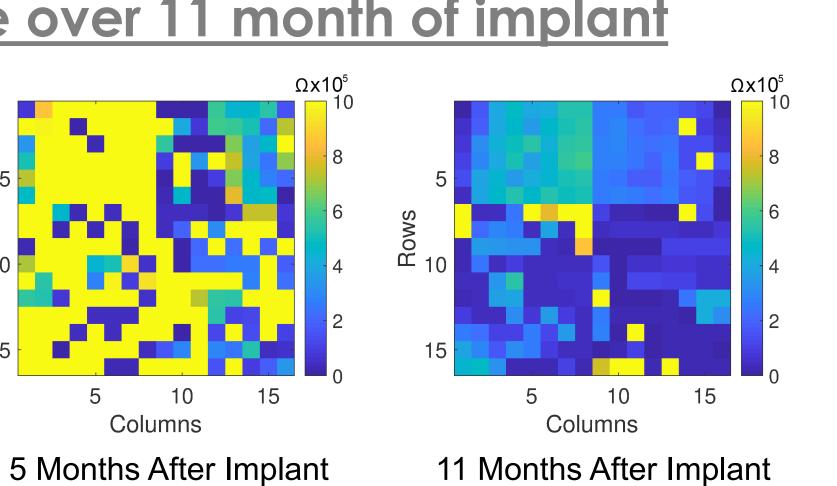


#### NHP EXPERIMENT

#### Subdural implant over vIPFC.

- . A monkey participated in a "cocktail-party" task that required him to detect a target vocalization that was embedded in a background chorus. Task difficulty was titrated by varying the soundlevel ratio between the target and the background chorus (TCr).
- 2. We recorded µECoG signals while the monkey participated in the task.

# Impedance over 11 month of implant



#### SIGNAL PROCESSING

Columns

1 Week After Implant

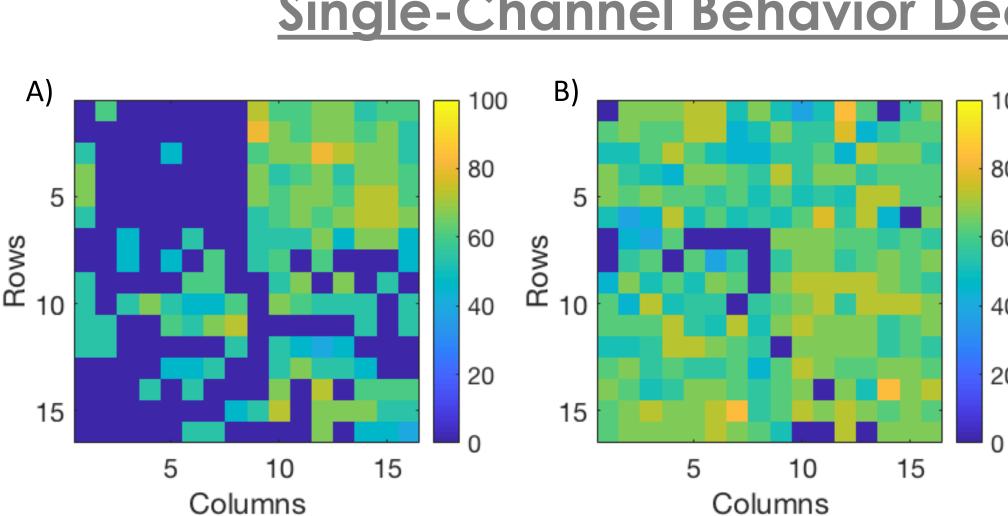
# Signal Processing Flow for SVM\*

- 1. Select features (mean, variance).
- 2. Calculate single-channel classification accuracy using SVM (LibSVM in the MATLAB platform)
  - a. Grid-search to optimize LibSVM parameters with Nfold cross-validation
- 3. Pick channels corresponding to top 20<sup>th</sup> percentile.
- 4. Run cross-validated SVM classification for 1, 2, 4, ..., N channels.

\*SVM: Support Vector Machine

# Single-Channel Behavior Decoding

Columns



- A) 5 month after implant
- B) 11 months after implant
  - Single channel accuracy
- is not stationary over time

#### DECODING RESULTS

#### Behavior Decoding (Hits v. Misses)

# **Broad Band** Gamma band 1 2 4 8 16 2 4 8 16 No. of Channels No. of Channels

# Sensory Decoding (Target-to-Chorus ratio)

# **Broad Band** Earliest Sess. 100 == Earliest Sess. No. of Channels No. of Channels

- 1. Solid lines: decode capacity; dotted lines: bootstrap null distribution; each set is decode from a single recording session; data in blue from earliest session; data in red from last recording session. Data in grey are from other sessions; the darker the shading the more recent the session.
- 2. Behavior decoding states: (a) Hits, (b) Misses, (c) False Alarm, and (d) Correct Rejection.
- 3. Sensory decoding states: 5 target-to-chorus ratios ranging from 60% to 80%.
- 4. Classification accuracy both for behavioral outcomes and TCr improved significantly as the number of decoding channels increased.
- 5. Higher frequency bands, such as gamma band, showed the most noticeable enhancement in decoding accuracy, relative to other bands (not shown).

#### DISCUSSION / SUMMARY

- μECoG signals in vIPFC code both behavioral outcomes and stimulus parameters.
- Sufficient coverage and recording resolution is needed:
- Individual channels varied significantly in their ability to decode various behavioral parameters (e.g., hits versus misses).
- For those channels that performed better than chance, as we increased the number of channels, decoding performance improved. This improvement was seen across a variety of neural frequency bands.

#### ACKNOWLEDGEMENTS

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